# Photobiomodulation guided healing in a sub-critical bone defect in calvarias of rats

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**Background:** Photobiomodulation presents stimulatory effects on tissue metabolism, constituting a promising strategy to produce bone tissue healing.

**Objective:** the aim of the present study was to investigate the in vivo performance of PBM using an experimental model of cranial bone defect in rats.

**Material and Methods:** rats were distributed in 2 different groups (control group and PBM group). After the surgical procedure to induce cranial bone defects, PBM treatment initiated using a 808 nm laser (100 mW, 30 J/cm², 3 times/week). After 2 and 6 weeks, animals were euthanized and the samples were retrieved for the histopathological, histomorphometric, picrosirius red staining and immunohistochemistry analysis.

**Results:** Histology analysis demonstrated that for PBM most of the bone defect was filled with newly formed bone (with a more mature aspect when compared to CG). Histomorphomeric analysis also demonstrated a higher amount of newly formed bone deposition in the irradiated animals, 2 weeks post-surgery. Furthermore, there was a more intense deposition of collagen for PBM, with ticker fibers. Results from Runx-2 immunohistochemistry demonstrated that a higher immunostaining for CG 2 week's post-surgery and no other difference was observed for Rank-L immunostaining.

**Conclusion:** This current study concluded that the use of PBM was effective in stimulating newly formed bone and collagen fiber deposition in the sub-critical bone defect, being a promising strategy for bone tissue engineering.

**Key words:** photobiomodulation  $\cdot$  low-level laser therapy  $\cdot$  bone healing  $\cdot$  calvarial bone defect.

# Introduction

The stimulatory effects of low-level laser therapy (LLLT) or more recently, photomobiomodulation (PBM) on biological tissues, have been highlighted for many studies <sup>1-4)</sup>, including the ability of modulating inflammatory processes after an injury, accelerating soft and hard tissue heal-

ing and stimulating neoangiogenesis <sup>5-7)</sup>. The action of PBM can be explained mainly by the interaction of laser light and tissues, which generates a series of modifications in cell metabolism. When PBM is applied to tissue, light is absorbed by chromophore photoreceptors located in the cells, stimulating the mitochondrial respiration, the production of molecular oxygen and ATP synthesis <sup>4,8-10)</sup>. These effects can lead to increased expression of genes related to protein synthesis, cell migration and proliferation, anti-inflammatory signaling, anti-apoptotic proteins and antioxidant enzymes. Also, stem cells and progenitor

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Based on these effects, this therapeutic intervention has been also used to stimulate bone metabolism and fracture consolidation <sup>13-16</sup>. Favaro-Pipi *et al.* <sup>17)</sup> showed that 830nm laser (50 W/cm², 50 J/cm², 30 mW) produced an increase in the expression of genes related to bone differentiation, mainly BMP4, ALP and Runx-2 expression in an experimental model of bone defects in rats, demonstrating that this treatment is able of improving bone healing. Moreover, microarray analysis demonstrated that PBM produced an upregulation of genes related to the inflammatory process (MMD, PTGIR, PTGS2, PTGER2, IL1, 1IL6, IL8, IL18) and angiogenic activities (FGF14, FGF2, ANGPT2, ANGPT4 and PDGFD) in an experimental model of tibial bone defects in rats <sup>1,18</sup>.

Although all the positive effects of PBM have already been demonstrated, most of the studies are performed using non-critical bone defects, which is a limiting factor. In this context, it is highly required the use of sub-critical and critical models, which can better simulate clinical conditions of non-union fractures and pseudarthrosis. In view of the aforementioned, it was hypothesized that the treatment of sub-critical bone defects with PBM would be able of accelerating tissue metabolism, stimulating bone healing. Consequently, the present study aimed to evaluate the biological temporal modifications (using 2 experimental periods) of PBM on newly formed bone using a 5mm cranial bone defect trough histological, histomorphometry and immunohistochemistry analysis.

## **Materials and Methods**

## In vivo study

Third -two male Wister rats (12 weeks, 300-350g) were used as experimental animals. All animals were submitted to the surgical procedure to perform the critical cranial size bone defects. Animals were randomly divided into 2 groups (n=16 per group): Control Group (CG) and PBM Group (PBM). Each group was divided into two subgroups, euthanized by  $\rm CO_2$  suffocation after 2- and 6-weeks post-surgery (n = 8 for each subgroup). All animals were maintained under controlled temperature (22  $\pm$  2°C), light–dark periods of 12 h and had free access to water and standard food. This study was approved by the Animal Care Committee guidelines of the Federal University of São Paulo (CEUA n° 9574290614).

## Surgical procedures

For the surgical procedures, rats were submitted to anaesthesia with a combination of ketamine (80 mg/kg), xylazine (8 mg/kg), acepromazine (1 mg/kg) and fentanyl (0.05 mg/kg). To insert implants, the animals were immobilized, and the skull was shaved, washed and disinfected

with povidone-iodine. Using aseptic techniques, an incision was made through the skin and the periosteum of the skull and a full-thickness flap was obtained. A 5 mm defect was created in the parietal region using a bone trephine drill (3i Implant Innovations Inc., Palm Beach Gardens, USA) under copious saline irrigation 19, 20). The preset implants were placed in the created defect, according to a randomization scheme. Thereafter, the wound was closed with resorbable Vicryl® 5-0 (Johnson & Johnson, St.Stevens-Woluwe, Belgium) after which the skin was also sutured with nylon (Agraven®; InstruVet BV, Cuijk, The Netherlands). Four animals were housed per cage and the intake of water and food was monitored in the initial post-operative period. Further, rats were given appropriate postoperative care and animals were observed for signs of pain, infection and proper activity.

#### PBM treatment

The treatment with PBM started immediately after the surgery with a Photon Lase III equipment (DMC, São Carlos, Brazil). PMB parameters are described in **Table 1**. The irradiation was performed at one point, above and in the centre of the created defect, by the punctual contact technique. Three applications per week were performed, in non-consecutive days, totalling 6 and 18 sessions, respectively 2 and 6 weeks.

#### Histopathology

After the euthanasia, the skull parts were collected and fixed in 10% buffer formalin (Merck, Darmstadt, Germany) for 48 h, decalcified in 4% ethylenediaminetetraacetic acid (EDTA) (Merck, Darmstadt, Germany) and embedded in paraffin blocks. Thin sections (5 µm) were prepared using a microtome (Leica Microsystems SP 1600, Nussloch, Germany). Three sections of each specimen were stained with haematoxylin and eosin (Merck, Darmstadt, Germany) and examined using light microscopy

**Table 1:** PBM parameters

Parameters				
Wavelength	808 nm (infrared)			
Laser frequency	Continuous output			
Optical output	100 mW			
Spot size	$0.028 \text{ cm}^2$			
Power density	3.57 W/cm <sup>2</sup>			
Dose	30 J/cm <sup>2</sup>			
Energy	0.84 J			
Time per point	8 s			
Application mode	Stationary in skin contact mode			

(Leica Microsystems AG, Wetzlar, Germany, Darmstadt-Germany) <sup>2, 21, 22)</sup>. The presence of inflammatory process, granulation tissue, newly formed bone and material degradation were qualitatively evaluated in the laminas. The analysis was performed in a blinded way (AMPM).

#### Histomorphomeric analysis

Samples were quantitatively scored by using the semi-automatic image-analysing OsteoMeasure System (Osteometrics, Atlanta, GA, USA). All amount of newly formed bone in all samples were quantified separately for each specimen in order to compare between the experimental groups. For that, it was used the following parameter: osteoblast number per tissue area (N.Ob/T.Ar, /mm²), bone volume fraction (BV/TV, %), percentage of bone surface occupied by osteoblast (Ob.S/BS), and biomaterial volume per tissue area (BM.V/TV, %). In addition, the analysis was performed by two experienced observers (CPG and JLSP), in a blinded way.

# Picrosirius red staining Qualitative analysis

For the qualitative analysis, the samples were dewaxed and rehydrated, still immersed in 0.1% picrosirius red solution (Sirius red 0.1 g dissolved into 100 mL saturated picric acid solution) for 60 minutes of staining. After that, the samples were washed for 5 minutes, restrained with Harris haematoxylin (Merck) for 10 second. Following, the slides were dehydrated with gradient alcohol, and finally treating with xylene solvent and sealing with entellan (Sigma). The morphology, amount, and distribution of the collagen were observed under a polarized light microscope (AxioVision, Carl Zeiss, Jena, Germany). Type I collagen fibers, under a polarized light microscope, appear as yellow, orange-red, or red thick fibers.

#### Quantitative analysis

For quantitative analysis, photomicrographs from sections stained with Picrosirius-were taken by using a microscope (Axioshop 40 microscope, Carl Zeiss, Germany) under polarized (Sirius red staining) light, at 200x magnification <sup>23</sup>). This method allows to assess the presence, thickness and organization of the collagen fibers. For measurement, 3 images were taken for each specimen and using the "Imagen J software" (resolution of 1360 x 1024), the degree of gray scale of all images (1 to 255) were measured (with the higher values indicating an increased deposition of collagen). The values were expressed in percentage of the intensity of pixels (%) <sup>24</sup>). The analysis was performed in a blinded way (AMPM)

## Immunohistochemistry analysis

For immunohistochemistry analysis, it was used the protocol described previously <sup>2, 21)</sup>, using the streptavidin–biotin-peroxidase method. Briefly, paraffin from the sections

was removed with xylene. Then, the specimens were rehydrated in graded ethanol and pre-treated with 0.01 M citric acid buffer (pH 6) in a steamer for 5 min. To inactivate the endogenous peroxidase was used hydrogen peroxide in phosphate-buffered saline (PBS) for 5 min and blocked with 5% normal goat serum in PBS for 10 min. Following, the primary antibody was incubated with anti-Runx-2 polyclonal (code: sc-8566, Santa Cruz Biotechnology, USA) at a concentration of 1:300, and anti-Rank-L polyclonal (code: sc-7627, Santa Cruz Biotechnology, USA) also at a concentration of 1:300. The primary antibodies were incubated overnight at 4°C. Then, it was used the biotin-conjugated secondary antibody anti-rabbit IgG (Vector Laboratories, Burlingame, CA, USA) at a concentration of 1:200 in PBS for 1 h. Afterwards, samples were incubated with avidin biotin complex conjugated to peroxidase for 45 min. To reveal the immunostaining was used 0.05% solution of 3-3'-diaminobenzidine solution and restained with Harris haematoxylin (Merck) for 10 second. Finally, the specimens were analysed through the qualitatively (presence and location of the immunomarkers) and semi-quantitatively assess by using a light microscopy (Leica Microsystems AG, Wetzlar, Germany) according to a previously described scoring scale from 1 to 4 (1 = absent (0% of immunostaining), 2 = weak (1 - 35%)of immunostaining), 3 = moderate (36 - 67%) of immunostaining), and 4 = intense (68 – 100% of immunostaining) 2, 15). The analysis was performed in a blinded way (AMPM).

#### Statistical analysis

Data were analysed and displayed in tables and graphs, and the values expressed as mean and standard deviation. In the statistical analysis, the distribution of variables was tested using the Shapiro-Wilk normality test. For the analysis of multiple comparisons, ANOVA was used with post hoc Tukey for parametric data and nonparametric data, the Kruskal-Wallis test was used with post hoc Dunn. The level of significance was set at 5 % (p  $\leq$  0.05). All statistical analyses were performed using GraphPad Prism version 6.01.

#### **Results**

## Histopathological analysis Two weeks

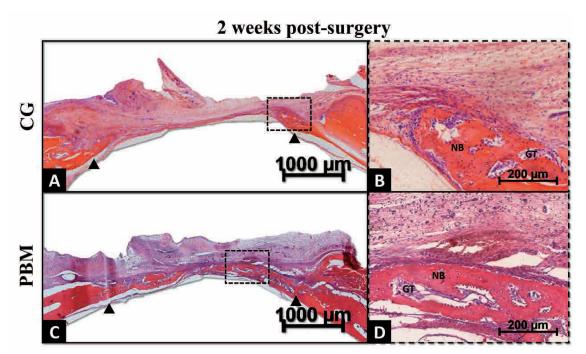
**Figure 1** shows a representative histological section of the experimental groups after 2 weeks post-surgery. In this experimental period, for CG, most of the defect was filled by granulation and conjunctive tissue, with some areas of newly formed bone at the borders of the defect **(Figure 1A and B)**. For PBM, granulation tissue was observed in most regions, with bone ingrowth being observed at the edges of the defect (surrounding the granu-

lation tissue). Also, some thick trabeculae from the borders to the centre region of the injury were presented (Figure 1C and D).

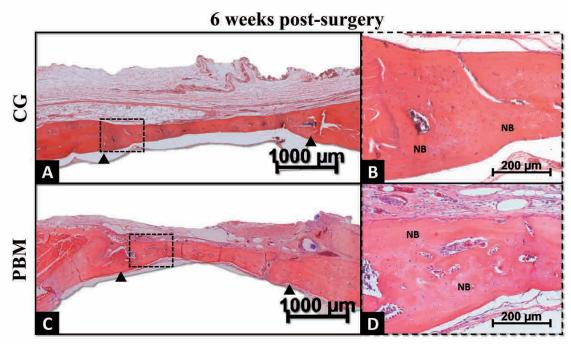
## Six weeks

An overview of the representative histological sections of

all experimental groups after a 6 weeks implantation period can be observed in **Figure 2**. For CG, newly formed bone was seen in all extension of the defect. In addition, no granulation or conjunctive tissue was observed **(Figure 2A and B)**. Similar histological patterns were observed for PBM treated animals, however, the tissue mor-



**Figure 1:** Representative histological sections of experimental groups. (A, B) CG; (C, D) PBM; after 2 weeks. NB - newly formed bone; RM – residual material. Hematoxylin and eosin. Scale bar = 1000 μm (mag. x2.5) and scale bar = 200 μm (mag. x20).



**Figure 2:** Representative histological sections of experimental groups. (A, B) CG; (C, D) PBM after 6 weeks. NB - newly formed bone; RM – residual material. Hematoxylin and eosin. Scale bar = 1000 μm (mag. x2.5) and scale bar = 200 μm (mag. x20).

phology seemed more mature, with thicker trabeculae compared to CG (Figure 2C and D).

## Histomorphometric analysis

**Table 2** shows the variables of the histomorphometric analysis. At 2 weeks post-surgery, for PBM, it was evidenced a higher value of BV/TV (p = 0.0076) and N.Ob / T.Ar (p = 0.0004) in comparison to CG. In the second experimental period was no difference between the groups.

# Picrosirius red staining analysis Qualitative analysis

**Figure 3** shows the photomicrographs of all experimental groups stained with picrosirius red, after 2 and 6

weeks of implantation. At 2 weeks post-surgery, CG and PBM, collagen fibers could be observed mainly at the borders of the bone defect **(3A and C)**. In the second experimental period, for CG, bone defect was filled with well interconnected collagen fibers **(Figure 3B)**. Similar findings were observed for PBM, which also presented connected fibers along the defect extension (thicker fibers compared to 2 weeks) **(Figure 3D)**.

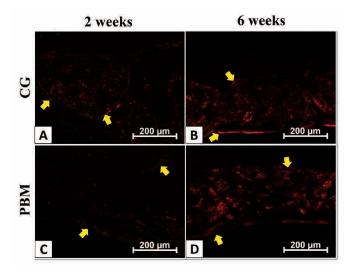
## Quantitative analysis

**Figure 4** shows the quantification of the presence of collagen through of the intensity of pixels. It is possible to observe that no difference was observed comparing both groups, at 2- and 6-weeks post-surgery.

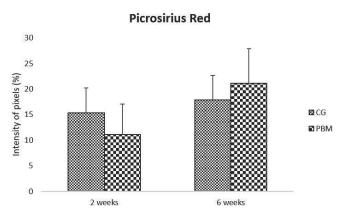
**Table 2:** Variables of the histomorphometric analysis 2- and 6-weeks post-surgery

Parameter	2 w	2 weeks		6 weeks	
	CG	PBM	CG	PBM	
Ob.S/BS (%)					
Mean	31.0	37.2	14.2	20.5	
SD	9.2	6.7	3.2	6.7	
N.Ob/T.Ar					
Mean	133.8	334.0	140.1	107.8	
SD	83.1	59.8	49.9	48.4	
BV/TV (%)					
Mean	12.7	26.6*	52.5	28.2	
SD	10.6	8.5**	9.1	16.1	

SD = standard deviation. \*PBM vs CG (2 weeks), p = 0.0076; \*\*PBM vs CG (2 weeks), p = 0.0004. Mann Whitney test.



**Figure 3:** Micrographs of picrosirius red stained bone sections with polarized light. (A, B) CG; (C, D) PBM after 2- and 6-weeks post-surgery, respectively. Picrosirius red stain. Scale bar = 200 μm (mag. x20).



**Figure 4:** Means and standard deviation of intensity of pixels of picrosirius red. BG/PLGA vs BG/PLGA/PBM (p = 0.0188). Dunn's test.

# Immunohistochemistry Runx-2 Qualitative analysis

Positive Runx-2 immunostaining was observed in all experimental groups 2 weeks post-surgery (**Figure 5**). For CG, Runx-2 immunostaining was observed mainly in the periosteum (**Figure 5A**). Furthermore, for PBM, Runx-2 immunostaining was seen mainly in the conjunctive tissue and in the newly formed bone (**Figures 5C**). At 6 weeks post-surgery, Runx-2 immunostaining was detected in few regions of the periosteum in CG and PBM (**Figure 5B and D**, respectively).

## Semi-quantitative analysis

**Figure 6** presented the semi-quantitative analysis of Runx-2 immunostaining. It is possible to observe a higher immunostaining for CG in comparison to PBM (p = 0.0069) at 2 weeks post-surgery. No difference was observed at 6 weeks post-surgery.

# Rank-L Qualitative analysis

**Figure 7** demonstrates the qualitative analysis of Rank-L immunostaining. At 2 weeks post-surgery, all experimental groups presented positive Rank-L immunostaining mainly in the conjunctive tissue and in newly formed bone (Figure 7A and C).

At 6 weeks post-surgery, Rank-L immunostaining for CG and PBM was noticed mainly in the periosteum and conjunctive tissue **(Figure 7B and D)**.

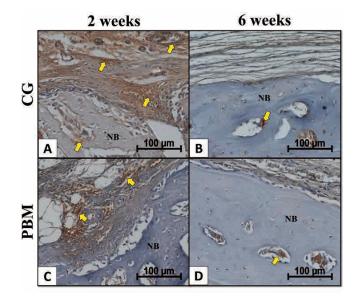
## Semi-quantitative analysis

**Figure 8** demonstrates the semi-quantitative analysis for Rank-L immunostaining. It is possible to observe that no difference was observed comparing both groups, at 2-and 6-weeks post-surgery.

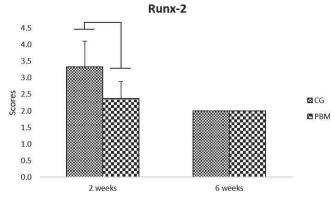
#### Discussion

In this study, the biological effects of PBM on bone healing in a sub-critical experimental model were evaluated. It was hypothesized that this therapy would be able of upregulating the immunostaining markers related to osteoblast differentiation, stimulating collagen and newly formed bone deposition. The main findings from the histological analysis showed that PBM treated animals presented a higher deposition of granulation tissue and newly formed bone in the area of the defect in both experimental periods. Also, the qualitative analysis of picrosirius staining demonstrated that the collagen fibers were ticker in the irradiated group. Runx-2 immunostaining presented higher values for CG 2 weeks post-surgery and no difference was observed for Rank-L immunostaining for both groups.

It is well known that PBM constitutes a promising effective therapeutic intervention able of stimulating bone tissue and producing healing <sup>1, 2, 25)</sup>. In the present study, histological findings demonstrated that PBM was able of stimulating newly bone deposition at the region of the defect. Many authors demonstrated that PBM was able of stimulating mesenchymal cells and osteoblasts, culminat-



**Figure 5:** Immunohistochemistry of Runx-2. CG (A, B); PBM (C, D); after 2- and 6-weeks post-surgery, respectively. Arrow indicates Runx-2 immunostaining. Scale bar = 100 µm.



**Figure 6:** Means and standard deviation of scores immunohistochemistry of Runx-2. 2 weeks: CG vs PBM, p = 0.0069. T test.

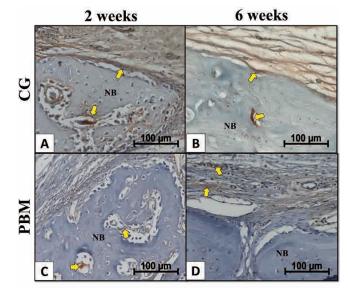
ing in the increase of newly formed bone deposition <sup>26-28)</sup>. Histomorphometry analysis corroborates the qualitative histological findings, presenting a higher value of BV/TV in the irradiated animals, 2 weeks post-surgery. The results of the present study may suggest that the energy from PBM was adequate to stimulate properly bone cells and consequently, increase the amount of newly formed bone. Shakouri et al. 29) showed that PBM enhanced the callus development in the early stage of the healing process in rabbits, with improvement in the biomechanical properties of bone healing. Also, PBM has been demonstrating to stimulate fracture bone healing in osteoporotic rats 30). Furthermore, it has been reported that PBM has a stimulatory effect on neovascularization by stimulating the secretion of angiogenic factors, which together with the osteogenic properties of PBM might further influence bone formation in the irradiated animals 31).

Moreover, both CG and PBM presented deposition of collagen fibers in the region of the defect, with thicker fibers being observed in the irradiated group, resembling a more mature tissue after 6 weeks post-surgery. It is known that collagen is the most found protein in the human body and the major component of organic matrix of bone tissue <sup>32, 33</sup>. During the process of fracture healing, an intense deposition of collagen matrix deposition is observed, which is, progressively, enriched with mineralized tissue <sup>34</sup>. For the present study, the thicker collagen fibers in the PBM treated animals, may indicate that the PBM possibly was able of anticipating cell recruitment and consequently, introducing earlier the normal phases of healing and the deposition of organic matrix, which may

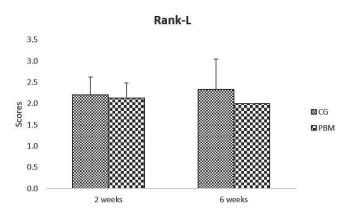
result in a mineralization and remodeling in the area of the defect <sup>34, 35)</sup>. These results are in agreement those of <sup>24)</sup> who also found a higher deposition of collagen fibers after PBM in a model of tibial bone defect in tibia of rats.

Additionally, Runx-2 is essential for the recruitment of mesenchymal cells to the osteoblast lineage and differentiation and maturation of osteoblasts 36, 37). Runx-2 influences the function of osteoblasts by regulating the expression of many osteoblast-related genes as ALP, OC, osteopontin and collagen type I 36, 37). The results of Runx-2 immunostaining from the present study demonstrated that CG presented higher values 2 weeks post-surgery. These findings may be explained by the set point analyzed after the surgical procedure (15 days). As it is known that PBM induces an earlier recruitment of stem cells and pre-osteoblastic cells 38), it is possible to suggest that the peak of Runx-2 synthesis may happen before 2 weeks in the irradiated group (in a period when the osteoblasts were more active). This hypothesis may be confirmed by the higher amount of newly formed bone in the defect area in the PBM group, indicating a higher activity of osteoblasts and consequently, a higher presence of Runx-2. This statement supports the idea that PBM shows an osteogenic potential. Interestingly, in the second experimental period, no difference was observed.

Similarly, Rank-L is regulator factor for osteoclast cell activation and it is involved with endochondral resorption and bone remodeling <sup>39, 40)</sup>. Interestingly, no difference in Rank-L immunostaining was observed between groups in both experimental periods. This fact suggests that PBM did not influence the amount of macrophages/



**Figure 7:** Immunohistochemistry of Rank-L. CG (A, B); PBM (C, D); after 2- and 6-weeks post-surgery, respectively. Arrow indicates Runx-2 immunostaining. Scale bar = 100 µm.



**Figure 8:** Means and standard deviation of scores immunohistochemistry of Rank-L T test.

osteoclasts bone tissue in the area of the defect and may imply that PBM stimulatory effects is related more to the stimulation of osteoblast acitivity. The findings of the present study corroborate those of Tim *et al.* <sup>15)</sup> who found no statistically significant difference in Rank-L immunostaining between CG and PMB 15, 30- and 45-days post-surgery in a model of tibial bone defect in rats. Patrocinio-Silva *et al.* <sup>41)</sup> also did not find any difference in Rank-L immunostaing after PBM in a model of tibial bone defect in diabetic rats.

In summary, this study revealed that PBM was able of stimulating newly formed bone and collagen fiber deposition, which indicate that this therapeutical intervention constitutes a promising treatment for bone tissue repair. Further long-term studies should be carried out to provide additional information concerning the application of PBM, especially in critical bone defects and compromised situations such osteoporosis.

#### Conclusion

The results of the present study support the notion that that PBM improved the process of bone repair in a sub-critical bone defect as a result of stimulation of the newly formed bone and increase of collagen fibers deposition. More studies should be developed to investigate the optimal parameters of PBM using critical models.

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## **Conflict of interest**

The authors declare no competing interests.

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